

Implant manual

 **SORIN** | INTENSIA DR 154

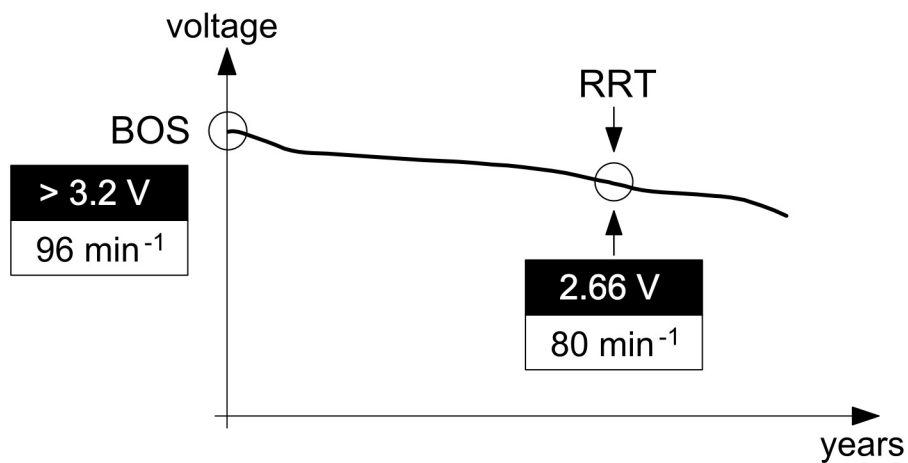


Implantable cardioverter defibrillator
DR model 154

SORIN INTENSIA DR 154

Reminder

Battery depletion



Leads connection

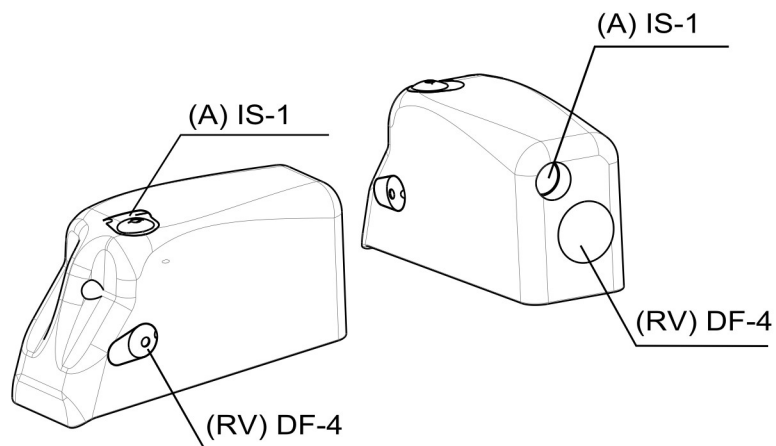


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1. GENERAL DESCRIPTION

INTENSIA DR 154 is an implantable dual-chamber cardioverter defibrillator. It is equipped with an accelerometer to allow adaptation of pacing to suit the patient's activity.

INTENSIA DR 154 is also equipped with the RF wireless technology which enables to remotely monitor the patients who have the Sorin SMARTVIEW Monitor installed at home.

INTENSIA DR 154 provides high energy shocks (42 J) for enhanced safety, as well as automatic lead measurements to monitor system integrity.

INTENSIA DR 154 is protected against high-frequency signals emitted by cellular telephones.

2. INDICATIONS

INTENSIA DR 154 is indicated for use in patients who are at high risk of sudden cardiac death due to ventricular tachyarrhythmias and who have experienced one of the following situations:

- Survival of at least one episode of cardiac arrest (manifested by the loss of consciousness) due to ventricular tachyarrhythmia,
- Recurrent, poorly tolerated sustained ventricular tachycardia (VT).

NOTE: The clinical outcome for hemodynamically stable VT patients is not fully known. Safety and effectiveness studies have not been conducted.

3. CONTRAINDICATIONS

Implantation of INTENSIA DR 154 is contraindicated in patients:

- whose ventricular tachyarrhythmias may have transient or reversible causes such as: acute myocardial infarction, digitalis intoxication, drowning, electrocution, electrolyte imbalance, hypoxia, sepsis, or unstable ischemic episodes,
- who present incessant tachyarrhythmia,
- who have an internal pacemaker,
- whose primary disorder is bradyarrhythmias, or atrial tachyarrhythmias.

Dual-chamber and single chamber atrial pacing is contraindicated in patients with chronic refractory atrial tachyarrhythmias.

4. WARNINGS AND PRECAUTIONS

The patient should be warned of the potential risks of defibrillator malfunction if he is exposed to external magnetic, electrical, or electromagnetic signals.

These potential interference sources may cause conversion to inhibited mode (because of noise detection), erratic delivery of VT or VF therapies, nominal programming, or much more rarely, irreversible damage to the device's circuits.

The main sources of high magnitude electromagnetic interference (EMI) are: powerful radiofrequency equipment (radar), industrial motors and transformers, induction furnaces, resistance, arc-welding equipment and high power loudspeakers.

Resuscitation Availability:

Do not perform device testing unless an external defibrillator and medical personnel skilled in cardiopulmonary resuscitation (CPR) are readily available.

Electrical Isolation:

Do not permit the patient to contact grounded equipment that could produce hazardous leakage current. Ensuing arrhythmia induction could result in the patient's death.

Disable the ICD During Handling:

Program Shock Therapy to OFF during surgical implant and explant or post mortem procedures. The device can deliver a serious high energy shock should accidental contact be made with the defibrillation electrodes.

Antitheft gates:

Since antitheft devices at the entrance to stores are not subject to any safety standards, it is advisable to spend as little time as possible in their vicinity.

Airport detection systems:

Since airport detection systems are not subject to any safety standards, it is advisable to spend as little time as possible in their vicinity.

High voltage power transmission lines:

High voltage power transmission lines may generate enough EMI to interfere with defibrillator operation if approached too closely.

Communication equipment:

Communication equipment such as microwave transmitters, linear power amplifiers, or high-power amateur transmitters may generate enough EMI to interfere with defibrillator operation if approached too closely.

Home appliances:

Home appliances that are in good working order and properly grounded do not usually produce enough EMI to interfere with defibrillator operation. There are reports of device disturbances caused by electric hand tools or electric razors used directly over the device implant site.



CAUTION: Do not tap sharply on the ICD can after implant, because the ICD's sensing circuits can detect this as P-waves or R-waves, and such oversensing could result in inappropriate pacing, inhibition, or therapy. Normal activities after implant do not result in such oversensing.

4.1. RISKS RELATED TO MEDICAL ENVIRONMENT

It is advisable to carefully monitor defibrillator operation prior to and after any medical treatment during which an electrical current from an external source passes through the patient's body.

Magnetic Resonance Imaging:

MRI is strictly contraindicated in cardiac defibrillator patients.

Radiofrequency ablation:

A radiofrequency ablation procedure in a patient with a generator may cause device malfunction or damage. RF ablation risks may be minimized by:

1. Programming Shock Therapy and ATP to OFF.
2. Avoiding direct contact between the ablation catheter and the implanted lead or generator.
3. Positioning the ground, placing it so that the current pathway does not pass through or near the device, i.e. place the ground plate under the patient's buttocks or legs.
4. Having external defibrillation equipment available.

Electrocautery or diathermy device:

Diathermy and electrocautery equipment should not be used. If such devices must be used:

1. Keep the current path and ground plate as far away from the device and the leads as possible (a minimum of 15 cm [six inches]).
2. Before procedure, disable ATP and shock therapies.
3. During the procedure, keep the electrocautery device as far as possible from the cardiac defibrillator. Set it at minimum intensity. Use it briefly.
4. After the procedure, check for proper implant function. The device should never be exposed directly to the diathermy source.

External defibrillation:

INTENSIA DR 154 is protected from external defibrillation shocks.

1. Before external defibrillation, disable ATP and shock therapies.
2. During external defibrillation, it is advisable to avoid placing the defibrillating paddles directly over the casing or over the leads. The defibrillating paddles should preferably be placed in an anteroposterior position.
3. Avoid any direct contact between the defibrillation paddles and the conductive parts of the implanted leads or casing of the implanted device.
4. After external defibrillation, check for proper device function.

Radiation therapy:

Avoid exposure to ionizing radiation. Betatrons are contraindicated. If high doses of radiation therapy cannot be avoided, the defibrillator should be protected from direct exposure with a protection shield. ATP and shock therapies should be disabled during exposure and proper device function should be checked regularly afterwards. Resulting damage may not be

immediately detectable. If irradiation of tissues close to the implantation site is necessary, it is recommended that the cardiac defibrillator be moved. As a safety measure, an external defibrillator should be immediately available.

Lithotripsy:

Lithotripsy may permanently damage the device if it is at the focal point of the lithotripsy beam. If lithotripsy must be used, keep the defibrillator at least 2.5 to 5 cm (1-2 inches) away from the focal point of the lithotripsy beam.

Diagnostic ultrasound (echography):

The defibrillator is not affected by ultrasound imaging devices.

Scales with body fat monitors and electronic muscle stimulators:

A patient with an implanted INTENSIA DR 154 should not use these devices.

4.2. STERILIZATION, STORAGE AND HANDLING

Resterilization:

Do not resterilize and re-implant explanted ICDs.

"Use Before" Date:

A "Use Before" date is printed on the outer storage package and on the sterile package. Do not implant the device after this date because the battery may have reduced longevity and sterility may be affected. It should be returned to Sorin.

If Package is damaged:

Do not use the device or accessories if the packaging is wet, punctured, opened or damaged because the integrity of the sterile packaging may be compromised. Return the device to the manufacturer.

Device Storage:

Store the device in a clean area, away from magnets, kits containing magnets, and sources of electromagnetic interference to avoid device damage. Store the device between 0 - 50 °C (32 - 122 °F). Temperatures outside the specified range may damage the device.

Equilibration:

Allow the device to reach room temperature before programming or implanting the device because rapid temperature changes may affect initial device function.

4.3. IMPLANTATION AND DEVICE PROGRAMMING

Use only a Sorin programmer to communicate with the device.

Do not inadvertently position any magnet over the ICD; this suspends tachyarrhythmia detection and treatment.

Replace the device when the RRT (Recommended Replacement Time*) point (defined by a battery voltage of 2.66 ± 0.01 V or a magnet rate lower than or equal to 80 bpm) is reached.

Program device parameters such as sensitivity threshold and VT and VF detection intervals as specified in the device manuals.

Lead System:

Do not use a lead system other than those with demonstrated compatibility because undersensing cardiac activity and failure to deliver necessary therapy may result.

In situations where an ICD and a pacemaker are implanted in the same patient, interaction testing should be completed. If the interaction between the ICD and the pacemaker cannot be resolved through repositioning of the leads or reprogramming of either the pacemaker or the ICD, the pacemaker should not be implanted (or should be explanted if previously implanted).

Failure to properly insert the torque screwdriver into the perforation at an angle perpendicular to the connector receptacle may result in damage to the sealing system and its self-sealing properties.

It is recommended that a security margin of at least 10 J be demonstrated between the effective shock energy and maximum programmable energy. Carefully confirm that true ventricular fibrillation has been induced because the DFT for ventricular tachycardia or flutter may be lower.

The defibrillator should be implanted with the engraved side facing outwards in order to facilitate telemetric communication with the programming head and to display the radiographic identification correctly.

*: corresponds to ERI (Elective Replacement Indicator) previously used.

4.4. LEAD EVALUATION AND LEAD CONNECTION

INTENSIA DR 154 has one IS-1, and one DF-4 connector ports.

IS-1 refers to the international standard whereby leads and generators from different manufacturers are assured a basic fit (ISO 5841-1:2000).

DF-4 refers to the international standard for defibrillation lead connectors (ISO 27186:2010).

Do not use the device with leads which have not been positively tested.

Do not tie a ligature directly to the lead body, tie it too tightly, or otherwise create excessive strain at the insertion site as this may damage the lead. Use the lead stabilizer to secure the lead lateral to the venous entry site.

Do not immerse the leads in mineral oil, silicone oil, or any other liquid.

Do not grip the lead with surgical instruments.

Do not use excessive force or surgical instruments to insert a stylet into a lead.

Use ventricular transvenous leads with caution in patients with either a mechanical or bioprosthetic tricuspid valvular prosthesis.

Use the correct suture sleeve (when needed) for each lead, to immobilize the lead and protect it against damage from ligatures.

Never implant the system with a lead system that has a measured shock impedance of less than 30 ohms. A protection circuit in the defibrillator prevents shock delivery when impedance is too low. If the shock impedance is less than 30 ohms, reposition the lead system to allow a greater distance between the electrodes.

Do not kink leads. Kinking leads may cause additional stress on the leads, possibly resulting in lead fracture.

Do not insert a lead connector pin into the connector block without first visually verifying that the setscrews are sufficiently retracted. Do not tighten the setscrews unless a lead connector pin is inserted because it could damage the connector block.

Lead electrodes in contact during a cardioversion or defibrillation therapy will cause current to bypass the heart, possibly damaging the ICD and the leads. While the ICD is connected to the leads, make sure that the metal portions of any electrodes do not touch each other.

If a pacing lead is abandoned rather than removed, it must be capped to ensure that it is not a pathway for currents to or from the heart.

If a thoracotomy is required to place epicardial patches, it should be done during a separate procedure to reduce the risk of morbidity and mortality.

Do not place the patch lead over nerve tissue as this may cause nerve damage.

Place the patch lead with the conducting coil side facing the heart to ensure delivery of energy to the heart.

Place the sutures well outside the coil of the patch lead or in the area between the coils to avoid possible coil fracture.

If countershock is unsuccessful using external paddles, adjust the external paddle position (e.g., anterior-lateral to anterior-posterior) and be sure that the external paddle is not positioned over the patch.

Do not fold, alter, or remove any portion of the patch as it may compromise electrode function or longevity.

If a header port is unused on the generator, the port must be plugged to protect the generator.

4.5. GENERATOR EXPLANT AND DISPOSAL

Interrogate the device, and program shock therapy off prior to explanting, cleaning or shipping the device to prevent unwanted shocks.

Return all explanted generators and leads to the manufacturer.

Never incinerate the device due to the potential for explosion. The device must be explanted before cremation.

5. ADVERSE EVENTS

Clinical data presented in this section are from the Defender and SafeR (AAI <> DDD) clinical studies. INTENSIA DR 154 is similar in design and function to the Defender devices. SafeR (AAI <> DDD) operation in INTENSIA is similar to that in the Symphony pacemaker. The data provided are applicable to INTENSIA DR 154.

5.1. DEFENDER STUDY

Clinical study of Defender IV DR 612 included 60 devices implanted in 60 patients, 38 in Europe (37 patients followed for a minimum of 3 months), and 22 in the U.S. (IDE G970282/S15) with a total device exposure of 228.7 and 30.3 device months, respectively. No deaths, serious adverse experiences or complications were judged to be device-related, as determined by the investigator. The following tables summarize the safety data for this study.

There was 1 death in the study that was classified as arrhythmic. The cause of death was recurrent VT/VF which occurred 19 days post implant.

In the following tables, complications are defined as adverse device effect, which cannot be treated or resolved by simple adjustments (e.g. reprogramming) and requires intervention.

NOTE: The company classified as complications those adverse device effects that were treated with surgery or with external defibrillation of a ventricular cardiac event.

Observations are defined as symptomatic or asymptomatic clinical events with potential adverse device effects that do not require intervention or can be corrected by simple adjustments.

NOTE: The company classified as observations those adverse device effects that were treated with programming changes, medication, or other method that was not classified as a complication.

Two of the 38 Defender IV DR 612 patients in Europe (37 patients followed for a minimum of 3 months) experienced a total of three complications, including device failures and replacements. Fourteen of the 38 Defender IV DR 612 patients experienced a total of 18 observations. Complications and observations are reported in Tables 1 and 2. It should be noted that a patient can have more than one observation or complication. There were no observations or complications in the U.S.

Table 1: Summary of European Clinical Complications

(Including Device Failures and Replacements)

All complications, 2 of 38 Defender IV DR 612 patients in Europe

Event	# of Patients	% of Patients	# of Events	Events/100 Device-Years*
Hematoma	1	2.6	1	5.2
Ventricular lead migration/dislodgment	2	5.3	2	10.5

* There were 228.7 device months in this study.

Table 2: Summary of European Clinical Complications

(Including Patient Complaints)

All complications, 14 of 38 Defender IV DR 612 patients in Europe

Event	# of Patients*	% of Patients	# of Events	Events/100 Device-Years**
Change in ventricular sensing threshold	1	2.6	1°	5.2
Device reset***	1	2.6	1°	5.2
Inappropriate therapy for EMI	1	2.6	1°	5.2
Pneumothorax	1	2.6	1°	5.2
Pocket hematoma	2	5.3	2°	10.5
Pocket infection/hematoma	1	2.6	1°	5.2
Pocket infection from previous pacemaker	1	2.6	1°	5.2
Prolonged implant procedure	1	2.6	1	5.2
Sensor acceleration during telemetry***	1	2.6	1	5.2
Shock for VT in VF Zone	1	2.6	1°	5.2
Slow VT not converted by ATP therapy	1	2.6	2°	10.5
Unsatisfactory sensing threshold test***	2	5.3	2	10.5
Ventricular oversensing	3	7.9	3	15.7

* A patient can have more than one observation.

** There were 228.7 device months in this study.

***These observations would not have happened with the currently marketed device and programmer.

°Investigator indicated that Defender IV DR did not cause or contribute to the event.

5.2. SAFER (AAI <> DDD) STUDY

Clinical study of the SafeR (AAI <> DDD) included 45 Symphony 2550 devices implanted in 45 patients. No serious adverse events were device- or feature-related. There were no deaths in the study.

Table 1: Summary of Symphony safety data during study

	Patients		Number of events	
	Number of patients	% of patients	Number of events	Events per device year ^(a)
Deaths	0	0	0	0
Explants	0	0	0	0
Serious pacemaker related events outside the use of SafeR (AAI <> DDD)	0	0	0	0

Non-serious pacemaker related events outside the use of SafeR (AAI <> DDD)	0	0	0	0
Serious events due to the use of SafeR (AAI <> DDD)	0	0	0	0
Non-serious events related due to the use SafeR (AAI <> DDD)	13	28.9	15	3.2
Serious non-pacemaker related events	6	13.3	9	1.9
Non-serious non-pacemaker related events	8	17.8	8	1.7

^(a) 4.74 device years

Non-serious events due to the use of SafeR 2 (AAI <> DDD) included: delay in switching on 2nd degree AV block, inappropriate classification of a PAC, disagreement between markers and recorded EGM, atrial pacing above the maximum rate, recycling on an R-wave in a refractory period, and disagreement in the statistics for switches to DDD. No patient symptoms were associated with these events.

6. CLINICAL STUDIES

Clinical data presented in this section are from the Defender and SafeR (AAI <> DDD) clinical studies. INTENSIA DR 154 is similar in design and function to the Defender devices. SafeR (AAI <> DDD) operation in INTENSIA is similar to that in the Symphony pacemaker. The data provided are applicable to INTENSIA DR 154.

6.1. DEFENDER STUDY

Objectives:

The primary objectives of this study were to demonstrate a complication free rate (CFR) comparable to that of historical controls, to demonstrate, using a chronotropic assessment exercise protocol (CAEP), a rate response proportional to and appropriate for the level of exercise, and to evaluate and report the incidence of adverse events.

Materials:

Each patient received one Defender IV DR 612 defibrillator, an atrial pacing and sensing lead, and a Medtronic, Angeion, or Biotronik defibrillation lead in the U.S. or any commercially available defibrillator lead outside the U.S.

Methods:

Investigators selected patients who survived at least one episode of cardiac arrest (manifested by loss of consciousness) presumably due to a ventricular tachyarrhythmia or exhibited recurrent, poorly tolerated, sustained ventricular tachycardia (VT). The protocol required evaluation of performance and adverse events at pre-discharge, one month, three months, six months, and (in the U.S.) every three months thereafter. At the one-month visit, eligible patients performed a chronotropic assessment exercise protocol (CAEP) maximal exercise test.

Study Population.

The table below summarizes inclusions.

Region	Date of first implant	Date of last implant	Data cut-off date	Number of centers	Number of patients
US	14-Dec-99	08-Mar-00	14-Mar-00	6	22
Europe	04-May-99	26-Jul-99	14-Apr-00	11	38
All	04-May-99	08-Mar-00	14-Apr-00 (Eur), 14-Mar-00 (US)	17	60

6.1.1 . Complication-free rate

Only European patients followed for at least 3 months:

Symbol	Parameter	Defender IV DR 612
N	Overall number of patients	37
Pe*N	Number of successes	35

Pe	Observed experimental proportion	0.95
Ps	Null hypothesis success rate	0.76
ES	Estimated standard error of Pe	0.04
z'	Test statistic ⁽¹⁾	4.75
p	Associated p-value	< 0,0001

(1) Statistical test: $z' = (Pe-Ps)/SE$ where $SE = \sqrt{Pe(1-Pe)/N}$

6.1.2 . Rate response

European patients only:

GROUP	Number of patients included	Mean slope %SRR on %MR	STD of slopes %SRR on %MR	SE of mean slope %SRR on %MR	Lower 95% CI	Upper 95% CI
Europe	20	0.77	0.17	0.04	0.69	0.84
Small Centers	9	0.79	0.18	0.06	0.67	0.91
Large Centers	11	0.75	0.15	0.05	0.66	0.84
Males	17	0.77	0.16	0.04	0.70	0.85
Females	3	0.73	0.22	0.13	0.47	0.98

SRR: Sensor Rate Reserve

MR: Metabolic Reserve

STD: Standard Deviation

SE: Standard Error

CI: Confidence Interval

6.1.3 . Adverse events

Event US (N=22)	Number of events*	Number of patients	Percent of patients
Intent to treat but did not	0	0	0.0
Non-device related death	0	0	0.0
Explant	0	0	0.0
Complication	0	0	0.0
Observation	0	0	0.0
Serious non-related other than death	1	1	4.5

Event Europe (N=38)	Number of events*	Number of patients	Percent of patients
Intent to treat but did not	0	0	0.0
Non-device related death	1	1	2.6
Explant	1	1	2.6
Complication	3	2	5.3
Observation	18	14	36.8
Serious non-related other than death	12	7	18.4

Event All (N=60)	Number of events*	Number of patients	Percent of patients
Intent to treat but did not	0	0	0.0
Non-device related death	1	1	1.7
Explant	1	1	1.7
Complication	3	2	3.3
Observation	18	14	23.3
Serious non-related other than death	13	8	13.3

* A patient can have more than one complication, observation, or serious adverse event, not device-related.

Device Failures and Replacements:

No device failures or replacements occurred with Defender IV DR 612 during the study.

6.2. SAFER (AAI <> DDD) STUDY

SafeR (AAI <> DDD) mode in INTENSIA is similar to that in Symphony.

The differences in SafeR (AAI <> DDD) mode between the two devices are:

- To prevent long RR intervals during VT/VF, SafeR (AAI <> DDD) has no effect during VT/VF therapy, electrophysiologic studies, and post-shock recovery.
- The maximum acceptable AV delay for first degree AV block varies as a function of pacing rate.
- INTENSIA requires a ventricular sensed event to atrial paced event (RA) interval of at least 100 ms. Therefore, the device lengthens the atrial escape interval so that it ends at least 102 ms after the ventricular event.
- During atrial fibrillation episode, pause criterion is fixed to 2s to avoid long bradycardia episodes in switching to DDD mode.

Despite these differences, the data collected on Symphony devices are applicable to INTENSIA because the principles of SafeR (AAI <> DDD) operation did not change. The

criteria for switching from AAI to DDD (or vice versa) did not change. The device's method for evaluating the presence of AV conduction did not change.

Methods:

All patients were implanted with a Symphony Model 2550 dual-chamber rate-responsive pacemaker with SafeR (AAI <> DDD) mode. A variety of marketed atrial and ventricular pacing leads were used. The pacemaker was programmed and interrogated via bi-directional telemetry using a Sorin dedicated programmer and a CPR3 programming head.

The study's routine evaluation consisted of enrollment, pre-discharge evaluation, and a scheduled follow-up visit at one month. At pre-discharge, a 24-hour Holter recording was performed and pacemaker memory was read. At one month, pacemaker memory was read. Investigators also documented adverse events.

Patients studied:

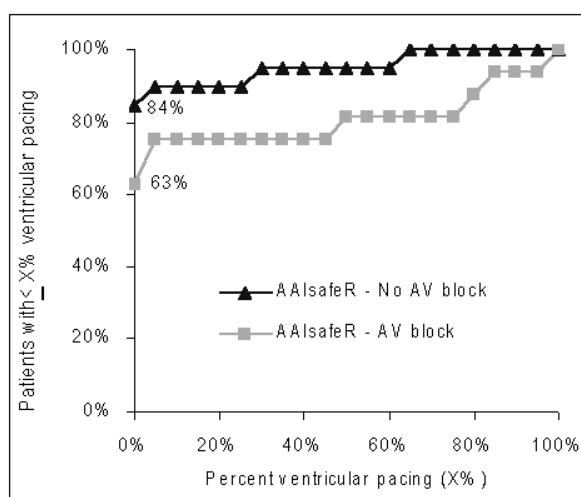
A total of 45 patients from 12 centers had Symphony 2550 pacemakers with SafeR (AAI <> DDD). Of these, 14 (31 %) were female and 31 (69 %) were male. Mean patient age (\pm SD) was 74 ± 9 years.

Primary indications for implant were: 1st degree AV block (11.1 %), 2nd degree AV block (6.7 %), 3rd degree AV block (22.2 %), sinus node dysfunction (62.2 %) or other (6.7 %).

Effectiveness results:

To determine the effectiveness of SafeR (AAI <> DDD) mode, the percentage of ventricular pacing provided over one month was recorded from pacemaker memory.

Thirty-five patients contributed data to evaluate the percentage of ventricular pacing provided with SafeR (AAI <> DDD). Twenty-nine patients had 1 % or less ventricular pacing and six patients had a range of 28-97 % ventricular pacing. The graph below shows the distribution of ventricular pacing observed in patients with and without AV block as a primary indication for implant.



The graph shows that many patients programmed to SafeR (AAI <> DDD) had less than 1% ventricular pacing:

- 84 % of patients without AV block at implant.
- 63 % of patients with AV block at implant.

In a representative reference group⁽¹⁾ of patients programmed to DDD, none had less than 1 % ventricular pacing and only 10 % had less than 90 % ventricular pacing regardless of AV block indication at implant.

The actual reduction of ventricular pacing that SafeR (AAI <> DDD) provides in an individual will depend on the amount of time that the patient spends in AV block. SafeR (AAI <> DDD) cannot and should not provide any decrease in ventricular pacing while the patient is in AV block.

⁽¹⁾ Pioger G, Jauvert G, Nitzsché R, Pozzan J, Laure H, Zigelman M, Leny G, Vandrell M, Ritter P, and Cazeau S. Incidence and predictive factors of atrial fibrillation in paced patients. *PACE*, 28, Supp 1: S137-141; January 2005. This was a prospective observational study of 377 patients with a functionally similar device programmed to DDD. The primary indications for implant were: AV block (49 %), sinus node disease (16 %), brady-tachy syndrome (5 %), AV block + sinus node disease (19 %), AV block + brady-tachy syndrome (6 %), and brady-tachy syndrome + sinus node disease (5 %).

Adverse events

Clinical study of the SafeR (AAI <> DDD) included 45 Symphony 2550 devices implanted in 45 patients. No serious adverse events were device- or feature-related. There were no deaths in the study. Table 1 summarizes the safety data for this study.

Table 1: Summary of Symphony safety data during study

	Patients		Number of events	
	Number of patients	% of patients	Number of events	Events per device year ^(a)
Deaths	0	0	0	0
Explants	0	0	0	0
Serious pacemaker related events outside the use of SafeR (AAI <> DDD)	0	0	0	0
Non-serious pacemaker related events outside the use of SafeR (AAI <> DDD)	0	0	0	0
Serious events due to the use of SafeR (AAI <> DDD)	0	0	0	0
Non-serious events related due to the use of SafeR (AAI <> DDD)	13	28.9	15	3.2
Serious non-pacemaker related events	6	13.3	9	1.9
Non-serious non-pacemaker related events	8	17.8	8	1.7

^(a) 4.74 device years

Non-serious events due to the use of SafeR 2 (AAI <> DDD) included: delay in switching on 2nd degree AV block, inappropriate classification of a PAC, disagreement between markers and recorded EGM, atrial pacing above the maximum rate, recycling on an R-wave in a refractory period, and disagreement in the statistics for switches to DDD. No patient symptoms were associated with these events.

7. PATIENT SELECTION AND TREATMENT

7.1. INDIVIDUALIZATION OF TREATMENT

Exercise stress testing:

If the patient's condition permits, use exercise stress testing to:

- Determine the maximum rate of the patient's normal rhythm,
- Identify any supraventricular tachyarrhythmias,
- Identify exercise-induced tachyarrhythmias.

The maximum exercise rate or the presence of supraventricular tachyarrhythmias may influence selection of programmable parameters. Holter monitoring or other extended ECG monitoring also may be helpful.



CAUTION: To avoid inappropriate therapy during an exercise stress test, do not reprogram any parameter during the test. When a parameter is reprogrammed, PARAD/PARAD+ algorithm forces acceleration to "ventricular". During conducted sinus tachycardia within the programmed Tachy zone, the device detects a 1:1 fast rhythm. Assuming that acceleration was set to ventricular by reprogramming, the device may identify this as a VT, and may immediately apply the corresponding therapy.

Electrophysiologic (EP) testing:

EP testing may be useful for ICD candidates.

EP testing may identify the classifications and rates of all the ventricular and atrial arrhythmias, whether spontaneous or during EP testing.

Drug resistant supraventricular tachyarrhythmias (SVTs):

Drug resistant supraventricular tachyarrhythmias (SVTs) may initiate frequent unwanted device therapy.

A careful choice of programming options is necessary for such patients.

Antiarrhythmic drug therapy:

If the patient is being treated with antiarrhythmic or cardiac drugs, the patient should be on a maintenance drug dose rather than a loading dose at the time of ICD implantation. If changes to drug therapy are made, repeated arrhythmia inductions are recommended to verify ICD detection and conversion. The ICD also may need to be reprogrammed.

Changes in a patient's antiarrhythmic drug or any other medication that affects the patient's normal cardiac rate or conduction can affect the rate of tachyarrhythmias and/or efficacy of therapy.

Direct any questions regarding the individualization of patient therapy to Sorin's representative.

7.2. SPECIFIC PATIENT POPULATIONS

Pregnancy:

If there is a need to image the device, care should be taken to minimize radiation exposure to the foetus and the mother.

Nursing Mothers:

Although appropriate biocompatibility testing has been conducted for this implant device, there has been no quantitative assessment of the presence of leachables in breast milk.

Pediatric Patients:

This device has not been studied in patients younger than 18 years of age.

Geriatric Patients:

Most of the patients receiving this device in clinical studies were over the age of 60 years.

Handicapped and Disabled Patients:

Special care is needed in using this device for patients using an electrical wheel chair or other electrical (external or implanted) devices.

8. PATIENT COUNSELLING INFORMATION

The physician should consider the following points in counselling the patient about this device:

- Persons administering CPR may experience tingling on the patient's body surface when the patient's ICD system delivers a shock.
- Advise patients to carry Sorin ID cards and/or ID bracelets documenting their ICD system.

9. CONFORMANCE TO STANDARDS

This device was developed in conformance with all or parts of the following standards:

- EN 45502-1: 1998 – Active implantable medical devices. General requirements for safety, marking and information to be provided by the manufacturer.
- EN 45502-2-1: 2003 – Active implantable medical devices. Part 2-1: Particular requirements for active implantable medical devices intended to treat bradyarrhythmia (cardiac pacemakers).
- EN 45502-2-2: 2008 – Active implantable medical devices. Part 2-2: Particular requirements for active implantable medical devices intended to treat tachyarrhythmia (includes implantable defibrillators).
- ISO 5841-3: 2013 Low profile connectors (IS1) for implantable pacemakers.
- ISO27186:2010 (DF-4): Active implantable medical devices - Four-pole connector system for implantable cardiac rhythm management devices — Dimensional and test requirements.
- ANSI/AAMI PC69: 2007 Active implantable Medical Devices - Electromagnetic compatibility - EMC test protocols for implantable cardiac pacemakers and implantable Cardioverter Defibrillators.
- IEC 60601-1-2 (2007): Electromagnetic compatibility - Medical electrical equipment. General requirements for basic safety and essential performance - Collateral standard.
- EN 50371 (2002): Generic standard to demonstrate the compliance of low power electronic and electrical apparatus with the basic restrictions related to human exposure to electromagnetic fields (10 MHz - 300 GHz).
- EN 301 489-1 (v1.8.1) & EN 301 489-27 (v1.1.1): Electromagnetic compatibility and Radio spectrum Matters (ERM); Electromagnetic Compatibility (EMC) standard for radio equipment and services - Part 1: Technical Requirements and Part 27: Specific conditions for Ultra Low Power Active Medical Implants (ULP-AMI) and related peripheral devices (ULP-AMI-P).
- EN 301 839-1 (v1.3.1) & EN 301 839-2 (v1.2.1): Electromagnetic compatibility and Radio spectrum Matters (ERM); Short Range Devices (SRD); Ultra Low Power Active Medical Implants (ULP-AMI) and Peripherals (ULP-AMI-P) operating in the frequency range 402 MHz to 405 MHz; Part 1: Technical characteristics and test methods and Part 2: Harmonized EN covering essential requirements of Article 3.2 of the R&TTE Directive.
- EN 62311 (2008): Assessment of electronic and electrical equipment related to human exposure restrictions for electromagnetic fields (0Hz to 300 GHz).
- EN 62209-2 (2010): Human exposure to radio frequency fields from hand-held and body-mounted wireless communication devices – Human models, instrumentation and procedures – Part 2: Procedure to determine the specific absorption rate (SAR) for wireless communication devices used in close proximity to the human body (frequency range of 30MHz to 6 GHz).

This information should not be used as a basis of comparisons among devices since different parts of the standards mentioned may have been used.

Sorin declares that this device is in conformity with the essential requirements of Directive 1999/5/EC on Radio and Telecommunications Terminal Equipment, with the mutual recognition of their conformity (R&TTE).

Federal Communication Commission Interference Statement 47 CFR Section 15.19 and 15.105(b)

The FCC product ID is **YSGDR154**.

This equipment has been tested and found to comply with the limits for a Class B digital device, pursuant to Part 15 of the FCC Rules. These limits are designed to provide reasonable protection against harmful interference in a residential installation. This equipment generates uses and can radiate radio frequency energy and, if not installed and used in accordance with the instructions, may cause harmful interference to radio communications. However, there is no guarantee that interference will not occur in a particular installation.

This device complies with Part 15 of the FCC Rules. Operation is subject to the following two conditions: (1) This device may not cause harmful interference, and (2) this device must accept any interference received, including interference that may cause undesired operation.

FCC Interference Statement 47 CFR Section 15.21 - No Unauthorized Modifications



CAUTION: This equipment may not be modified, altered, or changed in any way without signed written permission from SORIN. Unauthorized modification may void the equipment authorization from the FCC and will void the SORIN warranty.

Identification of the equipment according Section 95.1217(a)

This transmitter is authorized by rule under the Medical Device Radiocommunication Service (in part 95 of the FCC Rules) and must not cause harmful interference to stations operating in the 400.150-406.00 MHz band in the Meteorological Aids (i.e., transmitters and receivers used to communicate weather data), the Meteorological Satellite, or the Earth Exploration Satellite Services and must accept interference that may be caused by such stations, including interference that may cause undesired operation. This transmitter shall be used only in accordance with the FCC Rules governing the Medical Device Radiocommunication Service. Analog and digital voice communications are prohibited. Although this transmitter has been approved by the Federal Communications Commission, there is no guarantee that it will not receive interference or that any particular transmission from this transmitter will be free from interference.

IC Requirements for Canada

The IC product ID is **10270A-DR154**.

This class B digital apparatus meets all requirements of the Canadian Interference- causing equipment regulations.

This device complies with Industry Canada licence-exempt RSS standard(s). Operation is subject to the following two conditions: (1) this device may not cause interference, and (2) this device must accept any interference, including interference that may cause undesired operation of the device.

Under Industry Canada regulations, this radio transmitter may only operate using an antenna of a type and maximum (or lesser) gain approved for the transmitter by Industry Canada. To reduce potential radio interference to other users, the antenna type and its gain should be so chosen that the equivalent isotropically radiated power (e.i.r.p.) is not more than that necessary for successful communication.

This device may not interfere with stations operating in the 400.150–406.000 MHz band in the Meteorological Aids, Meteorological Satellite, and Earth Exploration Satellite Services and must accept any interference received, including interference that may cause undesired operation.

Cet appareil numérique de la classe B respecte toutes les exigences du règlement sur le matériel brouilleur du Canada.

Le présent appareil est conforme aux CNR d'Industrie Canada applicables aux appareils radio exempts de licence. L'exploitation est autorisée aux deux conditions suivantes: (1) il ne doit pas produire de brouillage, et (2) l'utilisateur du dispositif doit être prêt à accepter tout brouillage radioélectrique reçu, même si ce brouillage est susceptible de compromettre le fonctionnement du dispositif.

Conformément à la réglementation d'Industrie Canada, le présent émetteur radio peut fonctionner avec une antenne d'un type et d'un gain maximal (ou inférieur) approuvé pour l'émetteur par Industrie Canada. Dans le but de réduire les risques de brouillage radioélectrique à l'intention d'autres utilisateurs, il faut choisir le type d'antenne et son gain de sorte que la puissance isotrope rayonnée équivalente (p.i.r.e.) ne dépasse pas l'intensité nécessaire à l'établissement d'une communication satisfaisante.

Le présent dispositif ne doit pas causer de brouillage aux stations du service des auxiliaires de la météorologie, des satellites météorologiques, du service d'exploration de la terre par satellite, exploitées dans la bande 400,150-406,000 MHz, et il doit accepter tout brouillage reçu, y compris le brouillage pouvant entraîner un mauvais fonctionnement du dispositif.

10. PHYSICIAN GUIDELINES

10.1. PHYSICIAN TRAINING

Physicians should be familiar with sterile pulse generator implant procedure and familiar with follow-up evaluation and management of patients with an implantable defibrillator (or referral to such a physician).

10.2. DIRECTIONS FOR USE

ICD operating characteristics should be verified at the time of implantation and recorded in the patient file. Complete the *Patient Registration Form* and return it to Sorin, as it provides necessary information for warranty purposes and patient tracking.

Additional programming instructions can be found by accessing Online Help (click the “?” on the screen) on the Sorin dedicated programmer. Paper copies of Online Help can be obtained by contacting your Sorin representative.

10.3. MAINTAINING DEVICE QUALITY

This device is **FOR SINGLE USE ONLY**. Do not resterilize and reimplant explanted ICDs.

Do not implant the device when:

- It has been dropped on a hard surface because this could have damaged pulse generator components.
- Its sterility indicator within the inner package is not green, because it might not have been sterilized.
- Its storage package has been pierced or altered, because this could have rendered it non-sterile.
- It has been stored or transported outside the environmental temperature limits: 32 °F (0 °C) to 122 °F (50 °C) as an electrical reset condition may occur.
- "Use Before" date has expired, because this can adversely affect pulse generator longevity or sterility.

11. PATIENT INFORMATION

Information for the patient is available in the patient booklet, contained in the outer storage package. Additional copies can be obtained by contacting your Sorin representative or on the Sorin's web site: <http://www.sorin.com>.

This information should be given to each patient with their first ICD and offered to the patient on each return visit or as deemed appropriate.

12. HOW SUPPLIED

12.1. STERILITY

The INTENSIA defibrillators are supplied one per package in a sterile package.

12.2. WARRANTY AND REPLACEMENT POLICY

Sorin warrants its defibrillators. Refer to the section "Warranty" for additional information. Please see the following labelling sections for information concerning the performance of this device: Indications, Contraindications, Warnings and Precautions, and Adverse Events.

13. DEVICE DESCRIPTION

The INTENSIA DR system includes the model 154 ICD device and programming system. The programming system includes the Sorin dedicated programmer with the SMARTVIEW programming software connected to a CPR3 programming head. The programming system is configured and furnished by Sorin.

The INTENSIA DR 154 can serve as a defibrillation electrode (active housing) with a total surface area of 76 cm².

The INTENSIA DR 154 is designed to recognize and treat slow or fast VT and VF by continuously monitoring atrial and ventricular activity to identify persistent ventricular arrhythmias and to deliver appropriate therapies. INTENSIA DR 154 features the PARAD/PARAD+ algorithm, which is specifically designed to differentiate ventricular tachycardias from fast rhythms of supraventricular origin. PARAD/PARAD+ continuously monitors R-R interval stability, searches for long cycles, assesses the degree of P-R association, evaluates sudden onset and determines the chamber of arrhythmia acceleration.

In addition to the advanced detection scheme, INTENSIA DR 154 offers programmable dual or single-chamber pacing therapy (DDD, DDI, VVI or SafeR (AAI <> DDD) modes) with or without rate-responsive capabilities (DDDR, DDIR, VVIR, DDD/DDIR and SafeR-R (AAIR <> DDDR) modes) using an acceleration sensor. An automatic AV delay algorithm as well as a mode switching function are available.

INTENSIA DR 154 offers tiered therapy. Therapies can be programmed independently in each zone:

- in the Slow VT and VT zones: two ATP programs, up to two shocks with programmable energy and up to four shocks with maximum energy can be programmed;
- in the VF zone: one ATP program, up to two shocks with programmable energy and up to four shocks with maximum energy can be programmed.

When the rhythm changes from one zone to another, the device delivers the therapy programmed in this zone, starting with the same or more aggressive program for the area. The ATP program in the VF zone will only be applied if the VT coupling interval is longer than the programmed fast VT cycle length.

The INTENSIA DR 154 offers biphasic shocks with a maximum stored energy of 42 J. The shock configuration (electrodes used to apply the shock) can be chosen by programming one of the following combinations: can and one coil, can and two coils, two coils only.

Other features are as follows:

- Automatic ventricular sensitivity control
- Non-committed shocks
- Electrophysiological studies (EPS) with real-time markers or electrograms:
 - Programmer-controlled VT induction sequences,
 - Programmer-controlled VF inductions (30 Hz rapid pacing or shock on T),
 - Programmable electrogram vectors (EGM A, EGM V, RVcoil-CAN, SVC-CAN, RVcoil-SVC),
 - Real-time annotations displayed with the markers and indicating the majority rhythm,
 - Manual ATP sequences,
 - Manual shocks.

- Rescue shock
- Follow-up tests:
 - Pacing lead impedance,
 - Coil impedance,
 - Capacitor charge time,
 - Pacing threshold tests.
- Data storage:
 - Therapy History Report,
 - Statistics (pace/sense, therapy, shocks, and battery voltage),
 - Up to 14 complete Holter records with event logs, marker channel notation, and electrogram records.

The connector head has two ports:

- atrial bipolar pace/sense,
- one ventricular bipolar pace/sense and RV & SVC defibrillation coils.

Pace/sense port is compatible with the IS-1 standard and defibrillation ports is compatible with the DF-4 standard.

Distal lead terminal connections are secured with set-screws accessed via self-sealing silicone plugs. All lead connections pass through the header into the device via feedthroughs.

Programming System:

The Sorin programmer is used in conjunction with specific programmer software to interrogate and program the implanted device at implant and during patient follow-up procedures.

Remote Monitoring:

INTENSIA DR 154 is also equipped with the RF wireless technology which enables to remotely monitor the patients who have the Sorin SMARTVIEW Monitor installed at home.

14. IMPLANT PROCEDURE

14.1. NECESSARY EQUIPMENT

Implantation of INTENSIA DR 154 requires the following equipment:

- Sorin dedicated programmer, equipped with the SMARTVIEW software interface and with the programming head,
- pacing system analyzer, as well as its sterile connecting cables, to evaluate the pacing and sensing thresholds,
- a complete set of leads with corresponding introducers,
- physiological signal monitor capable of displaying simultaneously the surface ECG and arterial pressure,
- an external defibrillator with sterile external paddles,
- sterile cover for the telemetry head.



NOTE: In case you're implanting a DF-4 lead, please verify its compatibility with standard alligators pin; please refer to the lead user's manual for more details.

14.2. PACKAGING

14.2.1 . Contents

The INTENSIA DR 154 and its accessories are ethylene oxide sterilized and hermetically sealed in two-ply clear packaging meeting international requirements.

The sterile packaging contains a defibrillator and one screwdriver.

The non-sterile items contained in the outer storage package are the implant manual, the ICD Registration Form and its envelope, the patient booklet, the ICD ID card and 12 identification labels.

Once delivered, INTENSIA DR 154 is programmed to as-shipped values that are different from nominal values (see Chapter "Programmable Parameters" for details).

14.3. OPTIONAL EQUIPMENT

The following equipment may be required during implantation of INTENSIA DR 154:

- an IS-1 insulating plug to close the atrial port
- a DF-4/DF-1 adaptor in case of replacement and use of DF-1 lead
- sterile water to clean traces of blood. Any parts cleaned with sterile water must be thoroughly dried.
- mineral oil to lubricate if necessary
- a lead cap to isolate a lead which is not used

14.4. BEFORE OPENING THE PACKAGE

Before opening the package, check the "Use Before" date printed on the labels on the box and on the sterile package. Defibrillators that have not been implanted before that date should be returned to Sorin.

Interrogate the device:

- if a warning is displayed, do not implant the device and contact your Sorin representative.
- if magnet rate is lower than 91 min⁻¹, and if the last reforming/charge occurred more than one week ago, do not implant the device. Otherwise wait for one more week before checking the magnet rate again.

NOTE : The magnet rate and battery voltage can decrease before the expiration date is reached. However, the magnet rate should be equal to or higher than 91 min⁻¹ at the time of implant.

Devices MUST NOT be interrogated and programmed within the vicinity of other devices.

Also check the integrity of the sterile package. The sterility of the contents is no longer guaranteed if the package has been pierced or altered. If the defibrillator is no longer sterile, it should be returned in its packaging to Sorin. Any re-sterilization of the unit is at the discretion of Sorin.

14.5. PRIOR TO IMPLANTATION

Use the programmer to verify the defibrillator can be interrogated before implantation.

Verify all shock therapies are disabled in order to avoid accidental discharge during implantation.

It is not advisable to program the Smoothing function before implantation, since the defibrillator may detect noise and pace at a rate higher than the programmed basic rate.



CAUTION: Do not shake or tap sharply on the ICD package with the ICD inside, because the ICD's sensing circuits can interpret this as P-waves or R-waves and record these as an arrhythmia episode. If unusual shaking or tapping of the package results in a stored arrhythmia episode, erase the recording before using the ICD.

14.6. DEVICE PLACEMENT

The pocket should be prepared in the left pectoral position, either subcutaneously or submuscularly. Subcutaneous device implantation is recommended for optimal RF communication efficacy.

Implantation in an abdominal position is not advisable.

In its final position, the defibrillator should be no more than 4 cm below the skin surface.

14.7. CHOOSING THE TYPE OF LEAD

The defibrillator should be connected to:

- one bipolar atrial sensing/pacing lead
- one quadripolar/tripolar ventricular defibrillation lead with sensing/pacing bipolar electrodes, and one or two defibrillation electrodes.

The choice of leads and their configuration is left to the implanting physician's judgment.



NOTE1: Please note that DF-1 standard compliant lead is not compatible with DF-4 connector. In the opposite, DF-4 standard compliant lead is not compatible with DF-1 connector. In case of defibrillator replacement and use of a DF-1 lead or any other lead type that require an adaptor for this device, please contact your Sorin representative for any information on lead / connector compatibility question.

NOTE2: In case no atrial lead is implanted, the atrial port should be plugged with IS-1 insulating plug and a single chamber mode (VVI-VVIR) should be programmed. PARAD and PARAD+ should not be used.

Connectors:

The bipolar pacing/sensing connector is compatible with the IS-1 standard and the quadripolar connector is compatible with the DF-4 standard (refer to the "Lead evaluation and lead connection" sub-section in the "Warnings and precautions" section).

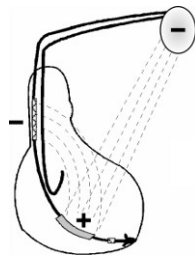
14.8. SHOCK CONFIGURATION (+ -> -)

The shock configuration is the energy pathway between the defibrillation electrodes. If an atrial coil is present, the shock configuration can be programmed for bi-directional shocks.

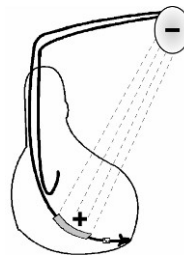
Programming:

When active case and SVC are both programmed to Yes, the shock configuration can be programmed to:

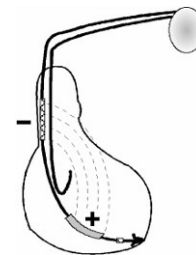
- RV to Case (or Case to RV),
- or RV to SVC (or SVC to RV),
- or RV to Case+SVC (or Case+SVC to RV).



RV to Case+SVC



RV to Case



RV to SVC

The polarity of shock is determined by the parameter itself.

14.9. MEASUREMENT OF THRESHOLDS AT IMPLANT

Pacing and sensing thresholds should be measured at implant.

Pacing thresholds:

Acute thresholds should be lower than 1 V (or 2 mA) for a 0.35 ms pulse width, both in the ventricle and in the atrium.

Sensing thresholds:

For proper ventricular sensing, the amplitude of the R-wave should be greater than 5 mV.

For proper atrial sensing, the amplitude of the P-wave should be greater than 2 mV.

Pacing impedance measurements:

Ventricular and atrial pacing impedances should range from 200 to 3000 ohms (refer to the lead characteristics, especially if high impedance leads are used).

14.10. LEAD CONNECTION

Implant the ventricular lead, then the atrial lead.

Each lead must be connected to the corresponding connector port. The position of each connector is indicated on the casing.



CAUTION:

Tighten only the distal inserts.

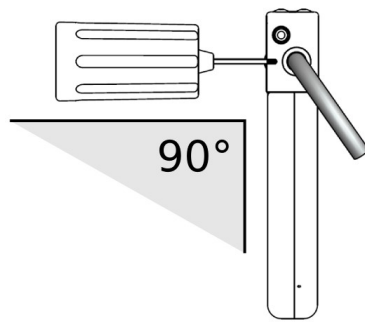
To connect each lead, proceed as follows:

1. Clean the lead terminal pins thoroughly, if necessary (device replacement).
2. Lubricate the lead terminal pins with sterile water, if necessary.
3. Do not insert a lead connector pin into the connector block without first visually verifying that the lead port is not filled with any obstacle.
4. Insert the screwdriver into the pre-inserted screw socket of the appropriate port (in order to allow excess air to bleed out and to make the insertion of the lead pin easier).
5. Insert the lead pin all the way into the port (check that the pin protrudes beyond the distal insert).
6. Tighten, check the tightness and ensure the lead pin still protrudes beyond the distal insert, and did not move.



CAUTION:

1. Do not tighten the pre-inserted screws when there is no lead (this could damage the connector).
2. Do not loosen the screws before inserting the connector (subsequent risk of being unable to reinsert the screw).
3. When mineral oil or sterile water is used to make lead insertion easier, the screwdriver should remain inserted into the pre-inserted screw socket when checking the tightness. As a matter of fact, when the lead port is filled with a liquid, the physics piston effect can give the feeling the lead is properly tightened.
4. One single set screw is located on the side of the connection header.
5. Use only the screwdriver provided with the defibrillator. Maintain the screwdriver's shaft perpendicular to the plane of the defibrillator (see figure below).
6. Removing the screwdriver: to avoid all risk of loosening screws during removal, hold the screwdriver by its metal part and not by the handle.



WARNING: Ensure that the screwdriver's tip is fully inserted in the setscrew; otherwise the screwdriver can damage the setscrew and prevent connection with or disconnection from the lead.

To ensure full insertion, push the screwdriver's hex tip smoothly into the setscrew until it reaches the bottom of the hex chamber in the screw, which could be felt as a solid metallic contact. Do not implant the defibrillator if there is no feeling of solid metallic contact. Do not implant the defibrillator if the wrench does not click when attempting to tighten the setscrew on the lead pin.



NOTE: To optimize cardioversion/defibrillation shocks, electrodes must be positioned so that the electric field between anode(s) and cathode covers the largest myocardial mass. In normal conditions, the anode and cathode are adequately separated. In case of a short-circuit, the shock may be aborted to prevent damaging the defibrillator.

In the case of an external defibrillation shock delivered to the patient, always check the programming and functioning of the device, in particular its capacity to deliver shocks.

14.11. DEVICE IMPLANTATION

INTENSIA DR 154 should be implanted with the engraved side facing outwards for optimal communication with the programming head and radiographic identification.

Carefully wind excess lead and place in a separate pocket to the side of the defibrillator.

It is recommended to not place any excess wire between the can and the heart.

Suture the casing connector to the muscle using the hole provided for this purpose, in order to avoid potential migration of the device into the pectoral muscle.

14.12. TESTS AND PROGRAMMING

During the implant testing procedure, it is recommended that a security margin of at least 10 J be demonstrated between the effective shock energy and maximum programmable energy.

Enable shock therapies, then program the defibrillator.

Verify that the defibrillation lead impedance for each shock delivered ranges from 30 to 150 ohms. Check the lead connection if the values are outside these boundaries.

Save the programming data on the programmer's hard disk and on an external storage device (if desired).

15. SPECIAL MODES

15.1. SAFETY MODE (NOMINAL VALUES)

Nominal values may be rapidly restored by pressing the following button on the programming head or programmer keyboard:



or via the Emergency button on the SMARTVIEW screen.

In safety mode, the defibrillator operates with the parameters underlined in the table of programmable parameters.

15.2. MAGNET MODE

When the magnet is applied:

- antiarrhythmia functions are inhibited (detection of rhythm disturbances, charging, and therapy),
- hysteresis and AVD paced/sensed offset are set to 0,
- pacing amplitude is set to 6 V,
- pulse width is set to maximum,
- pacing rate is set to the magnet rate,
- the following functions are disabled: ventricular arrhythmia prevention, Mode Switch, Anti-PMT, Smoothing, Rate Response.

When the magnet is removed:

- the sensor rate is forced to the basic rate,
- arrhythmia detection algorithms and sequential therapies are reinitialized,
- therapies start with the least aggressive program for each area.

The other parameters remain at their programmed value.

The magnet rate values are as follows:

Magnet rate (bpm)	96	94	91	89	87	85
Magnet period (ms)	625	641	656	672	688	703
Magnet rate (bpm)	83	82	80	78	77	
Magnet period (ms)	719	734	750	766	781	

15.3. RESPONSE IN THE PRESENCE OF INTERFERENCE

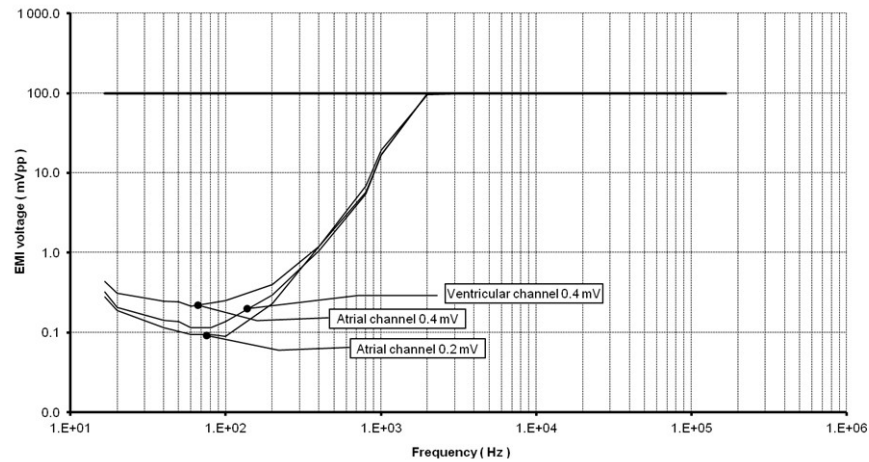
If the defibrillator senses electrical noise at a frequency above 16 Hz, it switches to an asynchronous mode at the basic rate. The programmed mode is restored as soon as the noise is no longer detected.

Ventricular pacing is also inhibited by ventricular noise. It can be restored by setting the parameter *V pacing on noise* to Yes.

15.4. DETECTION CHARACTERISTICS IN THE PRESENCE OF ELECTROMAGNETIC FIELDS

Per Clause 27.4 of Standard EN 45502-2-2, detection in the presence of electromagnetic fields is characterized as follows:

— Differential mode:



— Common mode rejection ratio:

	16.6 Hz	50 Hz	60 Hz
Atrial channel	≥ 75 dB	64 dB	62 dB
Ventricular channel	≥ 69 dB	≥ 57 dB	≥ 56 dB

Modulated interference:

For atrial sensitivity setting of 0.2 mV, compliance to the Cenelec standard 45502-2-2 is met for a maximum test signal amplitude of 8 V for the frequency of 60 MHz. 0.4 mV complies with the standard for the whole frequency range.

15.5. PROTECTION AGAINST SHORT-CIRCUITS

The defibrillator can undergo a short-circuit if the anode and cathode are not adequately separated.

In this case, the shock is aborted to prevent damaging the defibrillator and a warning will indicate that a short circuit (shock impedance < 20 ohms) was detected during the last shock.

16. MAIN FUNCTIONS

16.1. AUTOMATIC LEAD MEASUREMENTS

Automatic pacing lead impedance measurement:

A lead impedance measurement is automatically performed on atrial and ventricular leads every 6 hours. The daily mean impedance is stored for each chamber.

Automatic coil impedance measurement:

A coil impedance measurement is automatically performed on RV and SVC coils once a week. The result is stored in the device memory.

16.2. ATRIAL TACHYARRHYTHMIA MANAGEMENT

Mode Switch:

This function is designed to limit the acceleration and variation of ventricular rate in the presence of atrial arrhythmia.

16.3. VENTRICULAR TACHYARRHYTHMIA MANAGEMENT

Ventricular tachyarrhythmia prevention:

Set of algorithms that can be used to avoid the circumstances of ventricular tachyarrhythmia onset.

Searching for a long cycle (P And R based Arrhythmia Detection+: PARAD+):

Additional arrhythmia classification criterion to improve identification of atrial fibrillation and avoid inappropriate shocks.

Fast VT treatment:

Applies detection criteria on fast ventricular tachycardia that are different from those of the VT zone, as well as different therapies. The fast VT zone is included in the VF zone: its lower limit is determined by the programmed value for the VF zone and its upper limit by the programmed value for the fast VT zone.

Polarity alternation on Max shock:

Reverses the programmed polarity of every second shock set at maximum energy. The number, type, and energy of shocks is independently programmable by detection zone.

16.4. PACING

BTO (Brady Tachy Overlap):

Corrects chronotropic atrial incompetence by allowing pacing in the slow VT zone, without affecting arrhythmia detection specificity.

Post-shock mode:

After any automatic shock therapy, the post-shock mode makes it possible to apply a pacing mode other than the standard antibradycardia pacing mode and/or with different pacing parameters.

SafeR (AAI <> DDD) mode:

Is intended to minimize deleterious ventricular pacing. The defibrillator functions in AAI mode, and temporarily switches to DDD mode upon the occurrence of AVB III, AVB II, AVB I and ventricular pause.

Anti-PMT protection:

Is intended to protect the patient from Pacemaker-Mediated Tachycardia (PMT) without reducing atrial sensing capability of the device.

16.5. SENSING**Automatic Refractory Periods:**

Optimize sensing and make the implant programming easier. These periods are composed of a minimal Refractory Period and a triggerable Refractory Period. The duration of the refractory periods lengthens automatically as needed.

Committed period:

In DDI or DDD modes, the committed period is a non-programmable 95 ms ventricular relative refractory period that starts with atrial pacing. If a ventricular event is sensed during the committed period, but outside the blanking period, the ventricle is paced at the end of the committed period. The committed period prevents inappropriate ventricular inhibition if crosstalk occurs.

Protection against noise:

Allows the distinction between ventricular noise and ventricular fibrillation. If the device senses ventricular noise, the ventricular sensitivity is decreased until noise is no longer detected. Ventricular pacing can be inhibited to avoid a potential paced T-wave.

Automatic sensitivity control:

Optimizes arrhythmia detection and avoids late detection of T-waves and over-detection of wide QRS waves. The device automatically adjusts the sensitivities based on the ventricular sensing amplitude. In case of arrhythmia suspicion or after a paced event, the programmed ventricular sensitivity will be applied. The minimum ventricular sensitivity threshold is 0.4 mV (minimum programmable value).

16.6. FOLLOW-UP FUNCTION**Storage of memory data:**

AIDA+ (Automatic Interpretation for Diagnosis Assistance) software provides access up to 6 months of patient follow-up with day by day data collection, or up to 24 hours with hourly data collection. Episodes of ventricular tachyarrhythmia are recorded with the programmable EGM channels: either by selecting up to two traces, or by selecting "Double V" which enables a one-channel recording that is twice as long.

Diagnosis of AV conduction:

Automatic diagnosis of AV conduction with graphic displays.

Alerts / Warnings:

The device routinely performs security self-checks and technical measurements to ensure system integrity. When system integrity is found to be at risk outside a follow-up, alerts are stored in the device memory. When system integrity is found to be at risk during a follow-up, the information is managed as a warning (pop-up message) to notify immediately the user. For example, the following types of event can trigger a warning or an alert: technical problem during a shock, pacing lead impedance or coil impedance measurements out-of-range, battery depletion, ...

16.7. REMOTE MONITORING FUNCTION

Remote monitoring enables the automatic remote transmission of implant data to the physician thanks to the wireless Radio Frequency (RF) communication ability of the implant in order to provide a comprehensive report to the physician about device functioning and patient cardiac status without having the patient physically in the clinic.

The data is transmitted from the implant and the SMARTVIEW monitor, a small transmitter placed in the patient home.

Implant data are first transmitted to the SMARTVIEW monitor via RF. Data are then routed through the phone line to an internet website. This website is responsible for transforming the implant data into a comprehensive report that can be consulted by the physician.

16.7.1 . SMARTVIEW Monitor

The SMARTVIEW monitor is a small device equipped with an RF transmission module to communicate with the implant and a modem to export data through the internet.

The SMARTVIEW monitor is delivered to the patient who has to install it at home. Preferably the SMARTVIEW monitor will be placed on the nightstand of the patient, as close as possible to the side of the bed the patient usually sleeps. The SMARTVIEW monitor shall be connected to the phone line of the patient and the power plug. Regular transmissions are done during the night when the patient is asleep next to the SMARTVIEW monitor without any intervention from the patient.

16.7.2 . Transmission trigger

There are 3 different triggers for a remote transmission:

- the **remote follow-up transmission** is scheduled by the physician to occur regularly (according to the programming).
- the **alert transmission** will take place when the implant has recorded an abnormal event. The list of abnormal event is available in a following paragraph. Alert conditions are checked daily.
- the **on-demand follow-up transmission** is triggered by the patient himself through the use of a specific button on the remote-monitor.

16.7.3 . Data transmitted

The data transmitted are identical to the data available during a standard interrogation with the dedicated programmer. All counters, histograms, IEGMs and diagnosis available in the device are transmitted containing (not exhaustive list):

- programmed parameters
- Information on patient and system implanted

- battery status
- lead status (brady leads and defibrillation coils)
- pacing counters and mean heart rate (brady)
- atrial and ventricular arrhythmia counters and episodes
- ventricular therapy counters

Data are presented in the form of 2 reports to the physician: the first one contains a summary of major counters, histograms, warnings and diagnosis. The second one presents the 3 most important IEGM episodes automatically selected based on the degree of severity for the patient.

16.7.4 . User website

On the website, the physician is able to:

- consult and schedule the remote follow-ups of their patient
- configure additional ways of being notified of alerts (for instance by SMS, fax or e-mail)
- consult, print and export patient reports

16.7.5 . Alert system

The following set of alert trigger can be independently programmed ON/OFF by the physician using the dedicated programmer and can trigger an alert transmission:

- Low or high impedance (A, V)
- Abnormal coil impedance (shock lead)
- Low or High shock impedance
- Inefficient high energy shock
- All shocks programmed OFF
- Shock treated VT/VF
- Suspicion of noise on the V lead
- AF occurrence
- Fast V rate during AF



WARNING: The use of remote monitoring does not replace regular follow-up. Therefore, when using remote monitoring, the time period between follow-ups visits may not be extended.

17. PATIENT FOLLOW-UP

17.1. FOLLOW-UP RECOMMENDATIONS

Before the patient is discharged and at each subsequent follow-up visit, it is advisable to:

- check the occurrence of system warnings
- check the battery status,



NOTE: If the last reforming, charge or shock occurred during the week preceding the interrogation, the last battery value may be still impacted by the event. One week post event, the battery will recover its steady state value.

- check the integrity of the pacing and defibrillation leads,
- check for proper sensing (sensitivity, crosstalk) and pacing ; set the pacing amplitude to twice the pacing threshold,
- interrogate the implant memories (AIDA+),
- check the efficacy of the therapies delivered,
- keep a printout of programmed parameters, test results, and memory data,
- reset the memory data and statistics.

These operations should be performed by medical personnel in an appropriate care unit, with resuscitation equipment present.

It is recommended that a routine follow-up examination be done one month after discharge, and then every three months until the device nears the replacement date.

After a device reset, the magnet rate is equal to 87 bpm; it will be updated within the next 24 hours.

Refer to the online help for a description of displayed warning, and the necessity to contact Sorin for an evaluation.

Implant software upgrade:

In case a new implant software is downloaded in the device memory through the programmer, a warning message could be displayed by the programmer to inform the user and give the proper instructions to follow.

17.2. HOLTER FUNCTION

The Holter records up to 14 tachyarrhythmia episodes as well as the therapy history.

Stored Episodes

INTENSIA DR 154 stores up to 14 episodes (VF, VT, Slow VT, SVT/ST, non-sustained).

For each episode four levels of details are presented:

- Tachogram (to visualize PP and PR intervals)
- Event log for the entire episode:
 - PARAD/PARAD+ analysis for each majority,
 - Delivered therapies,

- Markers: Atrial and ventricular markers, sensed, paced and in relative refractory periods,
- EGM: onset and detection of the arrhythmia, on two therapies, and the return to slow rhythm by recording electrogram.

Therapy history

For each arrhythmia detection, each therapy delivered (either automatically or during an electrophysiological study) and at the end of each arrhythmia, INTENSIA DR 154 records the type of majority rhythm, the number of ATP sequences delivered, the energy and the number of shocks delivered.

17.3. RECOMMENDED REPLACEMENT TIME (RRT)

Recommended Replacement Time (RRT)⁽¹⁾ is controlled by:

- magnet rate equal to 80 ± 1 bpm or
- battery voltage equal to $2.66 \text{ V} \pm 0.01 \text{ V}$



CAUTION: The defibrillator should be replaced as soon as the Recommended Replacement Time (RRT) point is reached.

Between the RTT and the EOS (End of Service)⁽²⁾, INTENSIA DR 154 can still function for:

- 8.4 months (100% atrial and ventricular pacing in DDD mode, 500 ohms, with as-shipped settings), and deliver 7 shocks at 34 J or
- 6.4 months (0% pacing, sensors OFF, one 42 J shock every 2 weeks).

Once the Recommended Replacement Time (RRT) point has been reached, the device operates normally, except that the charge time increases. Under normal conditions (and without programmer use) the charge times are as follows:

	Shock energy	Charge time (sec)
BOS ⁽³⁾	42 J	10 (± 2)
RTT	42 J	13 (± 3)

(1) Recommended Replacement Time (RRT) corresponds to Elective Replacement Indicators (ERI) previously used.

(2) End of Service (EOS) corresponds to End of Life (EOL) previously used.

(3) Beginning of Service (BOS) corresponds to Beginning of Life (BOL) previously used.

17.4. EXPLANTATION

The defibrillator should be explanted in the following cases:

- The Recommended Replacement Time (RRT) point is reached
- Confirmed malfunction
- Burial of the patient (for environmental reasons, the local regulation may require the explantation of the devices containing a battery supply)
- Cremation of the patient (the defibrillator may explode if placed in an incinerator)

The explanted defibrillator should not be reused in another patient.

All explanted defibrillators should be returned to Sorin, carefully cleaned of all traces of contamination. This may be done by immersing them in an aqueous sodium hypochlorite containing at least 1% chlorine, followed by rinsing copiously with water.

The defibrillator should be protected against mechanical impact and the temperature variations that may occur during shipping.

Before explantation, it is advisable to:

- print out all programmed parameters, statistics and Holter function report,
- save Patient data on floppy disk or hard disk,
- disable shock therapies (VT and VF) to avoid any risk of untimely shock.

17.5. DEFIBRILLATOR IDENTIFICATION

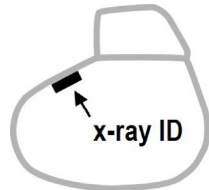
The defibrillator can be interrogated and programmed via telemetry, using the programming head interfaced with the Sorin dedicated programmer.

Position the programming head over the telemetry antenna located in the upper part of the device, in order to communicate effectively via telemetry (see diagram below).



The device can be non-invasively identified as follows:

1. Take an x-ray to identify the name of the manufacturer and model, printed on the device (X-ray ID is SDE : S = SORIN ; D = Defibrillator ; E = INTENSIA range).



2. Interrogate the device using the Sorin dedicated programmer. The model and serial number of the device are automatically displayed. The first figure in the serial number corresponds to the last figure in the year of manufacture.

18. PHYSICAL CHARACTERISTICS

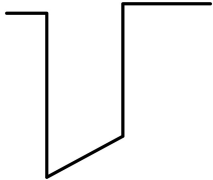

Dimensions	68.4 x 73.4 x 11 mm
Weight	95 g
Volume	38.6 cm ³
Active surface area of casing	76 cm ²
Connector	Atrium: IS-1. Ventricle: DF-4.

18.1. MATERIALS USED

Active surface area of casing	99% pure titanium
Connectors	Polyurethane* and silicone elastomer*

*Medical-grade materials that have undergone "in vitro" and "in vivo" qualifications.

19. ELECTRICAL CHARACTERISTICS

Atrial input impedance	80 kilohms \pm 30 %
Ventricular input impedance	80 kilohms \pm 30 %
D.C. capacitance	148 μ F \pm 8 %
Capacitor formation	No formation required
Rate limit	192 bpm \pm 10 bpm
Pacing waveform	
Defibrillation waveform	

19.1. TABLE OF DELIVERED SHOCK ENERGY AND VOLTAGE

The relationship between stored energies, maximum voltages and delivered energies (at 37 °C, 50 ohm load) for the minimum, low, mean and maximum programmed energy values is as follows:

Stored energy (J)	0.5	10	20	34	42
V1 (Volt)	75	341	483	631	702
V2 (Volt)	37	173	245	318	353
Delivered E: Phase 1 (J)	0.31	7.0	14.0	23.9	29.6
Delivered E: Phase 2 (J)	0.08	1.8	3.6	6.1	7.5
Delivered E: Total (J)	0.4	8.8	17.6	30.0	37.1

Tolerances are 12% for voltage (25% at 0.5 J) and 30% for energy.

19.2. BATTERY

Manufacturer	Greatbatch
Type	Quasar High Rate (QHR)
Model	GB 2593
Number of batteries	1

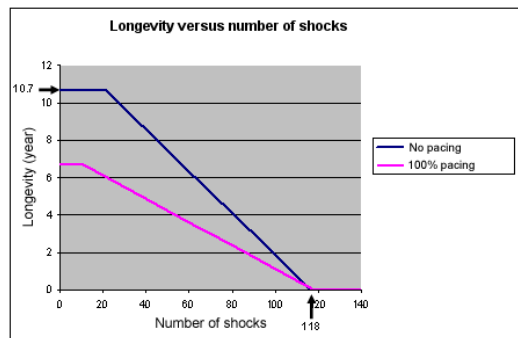
Total capacity	1964 mAh
Usable capacity	Between BOS and RRT: 1278 mAh. Between BOS and EOS: 1675 mAh.
Voltage	BOS: 3.25 V. RRT: 2.66 V. EOS: 2.5 V.

19.3. LONGEVITY

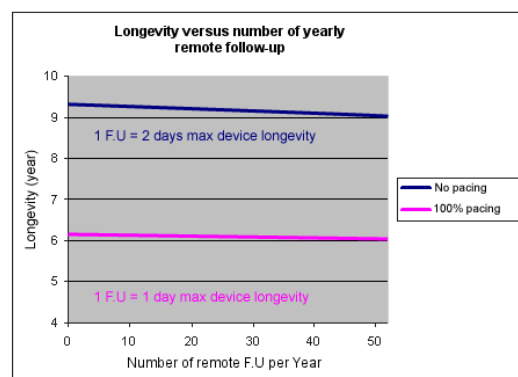
The longevities mentioned below are calculated by taking into account 6 months storage.

6.0 years	Pacing in DDD mode, 100%, 500 ohm, 3.5 V, 0.35 ms, 60 bpm, one 42 J shock per quarter, sensor OFF
5.8 years	Pacing in DDD mode, 100%, 500 ohm, 3.5 V, 0.35 ms, 60 bpm, one 42 J shock per quarter, G sensor ON
8.7 years	Pacing in DDD mode, 15% in atrium, 1% in ventricle, 500 ohm, 3.5 V, 0.35 ms, 60 bpm, one 42 J shock per quarter, sensor OFF
7.8 years	Pacing in DDD mode, 15% in atrium, 15% in ventricle, 500 ohm, 4.5 V, 0.50 ms, 60 bpm, one 42 J shock per quarter, sensor OFF
9.1 years	0% pacing, one 42 J shock per quarter, sensor OFF

The mean longevity as a function of shocks delivered at maximum energy, with and without pacing, is as follows:



The mean longevity as a function of yearly remote follow-ups⁽¹⁾, with and without pacing, is as follows:



(1) An excessive number of remote follow-ups can have a non-negligible impact on device longevity.

20. PROGRAMMABLE PARAMETERS

measured at 37 °C under a 500 ohm load

Legend:

Value in bold: "as shipped" value

Underlined value: nominal value

20.1. ANTIBRADYCARDIA PACING

Basic parameters	Values
Mode	<u>VVI</u> -VVIR-DDD-DDDR-DDD/DDIR-DDI-DDIR- SafeR (AAI <=> DDD) -SafeR-R (AAIR <=> DDDR)
Basic rate (bpm) ⁽¹⁾	From 30 to 90 by steps of 5 ; 60 (± 4 %)
Maximum rate (bpm)	From 100 to 145 by steps of 5 ; 120 (± 6 %)
Rate hysteresis (%)	<u>0</u> -5-10-20-35 (± 18 ms)
Rest AV delay (ms)	30-40-45-55-65-70-80-85-95-100-110-115-125-135-140-150- 155 -165-170-180-190-195-205-210-220-225-235-250 (± 19 ms)
Exercise AV delay (ms)	30-40-45-55-65-70- 80 -85-95-100-110-115-125-135-140-150-155-165-170-180-190-195-205-210-220-225-235-250 (± 19 ms)
AVD Paced/Sensed Offset (ms)	0-10-15-25-30-40-45-55- 65 -70-80-85-95-100-110-115-125 (± 1 ms)

(1) The corresponding periods are (in ms): 2000-1714-1500-1333-1200-1091-1000-923-857-800-750-706-667 ms.

Special features	Values
Smoothing	OFF -Very slow-Slow-Medium-Fast
Mode Switch	ON -OFF
Physical activity	Very low-Low- Medium -High-Very high

Pacing/Sensing	Values
Atrial sensitivity (mV) ⁽¹⁾	From 0.2 to 4 by steps of 0.2 ; 0.4 (± 50 %)
Atrial amplitude (V) ⁽²⁾	1-1.5-2-2.5-3- 3.5 -4-4.5-5-6 (± 20 %)
Atrial pulse width (ms)	0.12-0.25- 0.35 -0.5-0.6-0.75-0.85-1 (± 10 %)
Ventricular sensitivity (mV) ⁽¹⁾	From 0.4 to 4 by steps of 0.2 ; 0.4 (± 50 %)
Ventricular amplitude (V) ⁽²⁾	1-1.5-2-2.5-3- 3.5 -4-4.5-5-6 (± 20 %)
Ventricular pulse width (ms)	0.12-0.25- 0.35 -0.5-0.6-0.75-0.85-1 (± 10 %)

(1) Values are measured using a positive and negative triangular signal of 2/13 ms.

(2) The correlation between the programmed amplitudes, the stored amplitudes and the mid-pulse delivered amplitudes under a 500 ohm load are given in the following table:

Programmed ampl. (V)	1	1.5	2	2.5	3	3.5
Mid-pulse delivered ampl. (V)	0.97	1.39	1.79	2.35	2.84	3.25
Stored amplitude (V)	1.14	1.63	2.1	2.76	3.33	3.82
Programmed ampl. (V)	4	4.5	5	6		
Mid-pulse delivered ampl. (V)	3.58	4.23	4.47	5.37		
Stored amplitude (V)	4.2	4.96	5.25	6.3		

Ventricular arrhythmia algorithms	Values
Atrial pacing on PVC	Yes- No
Post extrasystolic pause suppression	Yes- No
Acceleration on PVC	Yes- No
Max acceleration rate (bpm)	From 60 to 145 by steps of 5 ; 100

Post-shock mode	Values
Mode	<u>OFF</u> -VVI-DDI- DDD
Duration	10s- 20s -30s-1min-2min-3min-4min-5min
Basic rate (bpm)	From 50 to 90 by steps of 5 ; 60 (± 4 %)
Rest AV delay (ms)	30-40-45-55-65-70-80-85-95-100-110-115-125-135-140-150- 155 -165-170-180-190-195-205-210-220-225-235-250 (± 19 ms)
Exercise AV delay (ms)	30-40-45-55-65-70- 80 -85-95-100-110-115-125-135-140-150-155-165-170-180-190-195-205-210-220-225-235-250 (± 19 ms)
AVD Paced/Sensed Offset (ms)	0-10-15-25-30-40-45-55- 65 -70-80-85-95-100-110-115-125 (± 1 ms)
A amplitude (V)	1-1.5-2-2.5-3- 3.5 -4-4.5-5-6 (± 20 %)
A pulse width (ms)	0.12-0.25- 0.35 -0.5-0.6-0.75-0.85-1 (± 10 %)
V amplitude (V)	1-1.5-2-2.5-3- 3.5 -4-4.5-5-6 (± 20 %)
V pulse width (ms)	0.12-0.25- 0.35 -0.5-0.6-0.75-0.85-1 (± 10 %)
Refractory periods	Values
Atrial refractory period post ventricular sensing (ms)	45 -65-80-95-110-125-140-155 (± 16 ms)
Atrial refractory period post ventricular pacing (ms)	80 -95-110-125-140-155 (± 4 ms)
Sensitivity margins	Values
Atrial post pacing/sensing margin (mV)	From 0 to 1 by steps of 0.2 ; 0.4
Ventricular post pacing margin (mV)	From 0 to 2 by steps of 0.2 ; 0.8
Response to noise	Values
Automatic sensitivity on noise	ON -OFF
V pacing on noise	ON- OFF
SafeR (AAI <=> DDD) parameters	Values
AVB I switch	Rest+Exercise -Exercise
Long PR: max (ms)	From 200 to 500 by steps of 50 ; 450
Long PR: min (ms)	From 200 to 500 by steps of 50 ; 250
Max. pause (s)	2-3 -4

20.2. VENTRICULAR TACHYARRHYTHMIA DETECTION

Therapy zones	Values
Slow VT detection zone ⁽¹⁾	Slow VT ON- Slow VT OFF
VT detection zone	VT ON- VT OFF
Fast VT / VF detection zone	Fast VT+VF ON- VF ON
Slow VT rate (lower limit) (bpm)	From 100 to 200 by steps of 5 ; 190
VT rate (lower limit) (bpm)	130-135-140-145-150-155-160-165-170-175-180-185- 190 -195-200-210-220-230
VF rate (lower limit) (bpm)	150-155-160-165-170-175-180-185- 190 -195-200-210-220-230-240
Fast VT rate (upper limit) (bpm)	155-160-165-170-175-180-185- 190 -195-200-210-220-230-240-255
Slow VT persistence (cycles)	4-6-8- 12 -16-20-30-50-100-200
VT persistence (cycles)	4-6-8- 12 -16-20-30-50-100-200
VF persistence (cycles)	From 4 to 20 by steps of 1 ; 6

(1) The Slow VT zone should be programmed ON only if the VT zone is programmed ON.

Detection criteria	Values
Slow VT and VT detection criteria	Rate Only-Stability-Stability+-Stability/Acc-Stability+/Acc- PARAD -PARAD+
Fast VT detection criteria	Rate+Stability -Rate Only
Majority: (X/Y), Y (cycles)	8 -12-16
Majority: (X/Y), X (%)	65-70- 75 -80-90-95-100
Window of RR stability for Slow VT and VT (ms)	30-45- 65 -80-95-110-125
Window of RR stability for fast VT (ms)	30 -45-65
Acceleration (%)	6-13-19- 25 -31-38-44-50
Long cycle persistence extension (cycles)	From 0 to 16 by steps of 1 ; 10
Long cycle gap (ms)	15-30-45-65-80-95-110-125-140-155- 170 -190-205
Atrial monitoring	Yes -No

20.3. VENTRICULAR TACHYARRHYTHMIA THERAPIES

Common parameters	Values
Enable ATP therapy	Yes- No
Enable shock therapy	<u>Yes</u> -No
Polarity alternation (42J)	Yes- No
Atrial coil (SVC) present	Yes -No
Active case	Yes -No
Shock configuration (+ --> -)	Case to RV-SVC to RV-Case + SVC to RV-RV to Case-RV to SVC- RV to Case + SVC
SVC exclusion (shock < 15J)	Yes- No

20.3.1 . Therapy parameters in slow VT zone

ATP 1 program	Values
ATP program	OFF -Burst-Burst+Scan-Ramp-Ramp+Scan
Number of sequences	1-2- 3 -4-5-6-7-8-9-10-11-12-13-14-15
Cycles in first sequence	1-2-3-4-5-6-7- 8 -9-10-11-12-13-14-15
Cycles added per sequence	0 -1-2-3-4-5-6-7-8-9-10-11-12-13-14-15
Coupling interval (%)	50-55-60-65-70-75- 80 -85-90-95
Ramp decrement (per cycle) (ms)	0 -4-8-12-16-20-30-40-50-60
Scan decrement (per sequence) (ms)	0-4- 8 -12-16-20-30-40-50-60
Time limit (min)	0.5 -1-1.5- 2 -2.5-3-3.5-4
Minimum cycle length (ms)	95-110-125-140-155-170-190-205- 220 -235-250-265-280-295-310

ATP 2 program	Values
ATP program	OFF -Burst-Burst+Scan-Ramp-Ramp+Scan
Number of sequences	1-2- 3 -4-5-6-7-8-9-10-11-12-13-14-15
Cycles in first sequence	1-2-3-4-5- 6 -7-8-9-10-11-12-13-14-15
Cycles added per sequence	0- 1 -2-3-4-5-6-7-8-9-10-11-12-13-14-15
Coupling interval (%)	50-55-60-65-70-75-80- 85 -90-95
Ramp decrement (per cycle) (ms)	0-4- 8 -12-16-20-30-40-50-60
Scan decrement (per sequence) (ms)	0 -4-8-12-16-20-30-40-50-60
Time limit (min)	<u>0.5</u> -1-1.5- 2 -2.5-3-3.5-4
Minimum cycle length (ms)	95-110-125-140-155-170-190-205- 220 -235-250-265-280-295-310

Shock program	Values
Shock 1 (J)	OFF -0.5-0.8-1-1.3-1.5-2-2.5-3-3.5-4-5-6-7-8-9-10-12-14-16-18-20-22-24-26-28-30-32-34-42
Shock 2 (J)	OFF -0.5-0.8-1-1.3-1.5-2-2.5-3-3.5-4-5-6-7-8-9-10-12-14-16-18-20-22-24-26-28-30-32-34-42
Number of Max. Shock (42 J)	OFF -1-2-3-4

20.3.2 . Therapy parameters in VT zone

ATP 1 program	Values
ATP program	OFF-Burst- Burst+Scan -Ramp-Ramp+Scan
Number of sequences	1-2- 3 -4-5-6-7-8-9-10-11-12-13-14-15
Cycles in first sequence	1-2-3-4-5-6-7- 8 -9-10-11-12-13-14-15
Cycles added per sequence	0 -1-2-3-4-5-6-7-8-9-10-11-12-13-14-15
Coupling interval (%)	50-55-60-65-70-75- 80 -85-90-95
Ramp decrement (per cycle) (ms)	0 -4-8-12-16-20-30-40-50-60
Scan decrement (per sequence) (ms)	0-4- 8 -12-16-20-30-40-50-60
Time limit (min)	<u>0.5</u> -1-1.5- 2 -2.5-3-3.5-4
Minimum cycle length (ms)	95-110-125-140-155-170-190-205- 220 -235-250-265-280-295-310

ATP 2 program	Values
ATP program	OFF-Burst-Burst+Scan- Ramp -Ramp+Scan
Number of sequences	1-2- 3 -4-5-6-7-8-9-10-11-12-13-14-15
Cycles in first sequence	1-2-3-4-5- 6 -7-8-9-10-11-12-13-14-15
Cycles added per sequence	0- 1 -2-3-4-5-6-7-8-9-10-11-12-13-14-15
Coupling interval (%)	50-55-60-65-70-75-80- 85 -90-95
Ramp decrement (per cycle) (ms)	0-4- 8 -12-16-20-30-40-50-60
Scan decrement (per sequence) (ms)	0 -4-8-12-16-20-30-40-50-60
Time limit (min)	0.5 -1-1.5- 2 -2.5-3-3.5-4
Minimum cycle length (ms)	95-110-125-140-155-170-190-205- 220 -235-250-265-280-295-310

Shock program	Values
Shock 1 (J)	OFF -0.5-0.8-1-1.3-1.5-2-2.5-3-3.5-4-5-6-7-8-9-10-12-14-16-18-20-22-24-26-28-30-32-34-42
Shock 2 (J)	OFF -0.5-0.8-1-1.3-1.5-2-2.5-3-3.5-4-5-6-7-8-9-10-12-14-16-18-20-22-24-26-28-30-32-34-42
Number of Max. Shock (42 J)	OFF-1-2-3- 4

20.3.3 . Therapy parameters in fast VT / VF zone

ATP 1 program	Values
ATP program	OFF- Burst -Burst+Scan-Ramp-Ramp+Scan
Number of sequences	1 -2-3-4-5-6-7-8-9-10-11-12-13-14-15
Cycles in first sequence	1-2-3-4-5-6-7- 8 -9-10-11-12-13-14-15
Cycles added per sequence	0 -1-2-3-4-5-6-7-8-9-10-11-12-13-14-15
Coupling interval (%)	50-55-60-65-70-75- 80 -85-90-95
Ramp decrement (per cycle) (ms)	0 -4-8-12-16-20-30-40-50-60
Scan decrement (per sequence) (ms)	0 -4-8-12-16-20-30-40-50-60
Time limit	10s-20s- 30s -1min-1.5min-2min
Minimum cycle length (ms)	95-110-125-140-155-170-190- 205 -220-235-250-265-280-295-310

Shock program	Values
Shock 1 (J)	OFF -0.5-0.8-1-1.3-1.5-2-2.5-3-3.5-4-5-6-7-8-9-10-12-14-16-18-20-22-24-26-28-30-32-34-42
Shock 2 (J)	OFF -0.5-0.8-1-1.3-1.5-2-2.5-3-3.5-4-5-6-7-8-9-10-12-14-16-18-20-22-24-26-28-30-32-34-42
Number of Max. Shock (42 J)	1-2-3- 4

20.4. REMOTE ALERTS AND WARNINGS

The device routinely performs security self-checks and technical measurements to ensure system integrity. When system integrity is found to be at risk outside a follow-up, alerts are stored in the device memory. When system integrity is found to be at risk during a follow-up, the information is managed as a warning (pop-up message) to notify immediately the user. For example, the following types of event can trigger a warning or an alert: technical problem during a shock, pacing lead impedance or coil impedance measurements out-of-range, battery depletion, etc. The Remote tab presents an overview of all the alerts managed by the device.

General parameters	Values
RF communication ⁽¹⁾	ON-OFF
Remote alerts ⁽¹⁾	ON-OFF

(1) RF and Remote alerts are turned on automatically if Shocks are programmed ON.

When Alerts are programmed "On", the following System Alerts are automatically activated:

- Battery depletion – RRT
- Device reset
- Excessive charge time (>25s)
- System integrity

Lead Alerts	Values
Abnormal A lead impedance	ON-OFF
Abnormal A lead low limit (Ohm)	200 -250-300-350-400-450-500
Abnormal A lead high limit (Ohm)	1500-1750-2000-2500- 3000
Abnormal V lead impedance	ON-OFF
Abnormal V lead low limit (Ohm)	200 -250-300-350-400-450-500
Abnormal V lead high limit (Ohm)	1500-1750-2000-2500- 3000
Abnormal RV coil impedance	ON-OFF
Abnormal SVC coil impedance	ON-OFF
Abnormal Shock impedance ⁽¹⁾	ON-OFF

(1) Normal impedance range [20 Ohm-200 Ohm]

Clinical status	Values
V oversensing	ON- OFF
High AT/AF burden	ON- OFF
AT/AF limit (on 24h) (h)	0.5-1-3- 6 -12-24
Fast V Rate during AT/AF	ON- OFF
Fast V Rate limit (bpm)	80-90- 100 -110-120
Fast V Duration limit (h)	0.5- 1 -3-6-12-24

Therapy information	Values
Shock disabled	ON -OFF
Shocks delivered	OFF-All shocks-Inefficient shock- Inefficient max shock

21. NON PROGRAMMABLE PARAMETERS

Interval	Values
Committed period	95 ms (\pm 5 ms)

Atrial refractory periods	Values
Post atrial sensing	47 ms (\pm 16 ms)
Post atrial pacing	109 ms (\pm 4 ms)

Ventricular refractory periods	Values
Post ventricular sensing	95 ms (\pm 16 ms)
Post ventricular pacing	220 ms (\pm 4 ms)
Post atrial pacing (blanking)	16 ms (\pm 3 ms)

Tachycardia criteria	Values
Window of PR association	63 ms (\pm 1 ms)

Therapies	Values
Waveform ⁽¹⁾	Constant tilt (50% - 50%)
Stored energy for the Max. shock	42 J
Pacing amplitude during ATP therapies	7 V (Actual value at 300 ms: 5.3 V)
Anti-PMT protection	Termin

(1) The device has 50% tilt in each phase thus delivers 94% of stored energy. Each phase is limited to 10 ms duration.

22. LIMITED WARRANTY

The INTENSIA implantable cardioverter defibrillator is the result of highly advanced research and all components have been selected after exhaustive testing.

Sorin Group Italia S.r.l. (identified as “Sorin” hereafter) guarantees the product INTENSIA against any damage caused by component failure or production defects during a period of four years after the implantation date, and Sorin commits itself to replace all INTENSIA devices according to the terms described in article 1 and described in article 2 of this section.

Sorin makes no claim that the human body will not react unsuitably to the implantation of the INTENSIA device, or that failure will never occur.

Sorin does not guarantee the suitability of INTENSIA in defined types of patients; selection of the device is a medical decision.

Sorin shall not be held liable for any damage indirectly associated with the INTENSIA, whether as part of normal or abnormal operation, nor damage from its explantation or replacement.

Sorin does not authorise anyone to modify these limited warranty conditions.

22.1. ARTICLE 1 : TERMS OF LIMITED WARRANTY

1. The INTENSIA implantable cardioverter defibrillator is only guaranteed for the first implantation.
2. The EURID/Eucomed implant form must be sent to Sorin within 30 days after implantation.
3. The INTENSIA cardioverter defibrillator must be implanted prior to the use-before date indicated on the packaging.
4. The limited guarantee only applies to suspect devices returned to the manufacturer, carefully packed and accompanied by an explantation report duly completed by the hospital or the doctor and considered defective after analysis by Sorin.

The device must be returned within the 30 days following explantation to Sorin.

Any device returned and replaced under the terms of this limited warranty will become the exclusive property of Sorin.

Any rights under the terms of this limited warranty will be forfeited if the INTENSIA device has been opened by anyone other than Sorin.

These rights will also be forfeited if the device has been damaged by carelessness or accident.

This is the case especially if the device has been exposed to temperatures above 50°C, to electrical abuse or to mechanical shock, particularly as a result of being dropped. Consequently, any expert opinion offered by a third party after the device has been removed also nullifies the guarantee.

5. The limited warranty will be forfeited if it is proven that the device has been misused or inadequately implanted, against the physicians' manual recommendations of INTENSIA.
6. The limited warranty does not include leads and other accessories used for the implantation.
7. The replacement terms or conditions described in article 2 include all devices that shall be replaced within the limited warranty period because of battery depletion, without any

link to a component failure or a production hazard. The device battery longevity varies with the type and number of delivered therapies.

8. Legal requirements of jurisdictions where the INTENSIA device is distributed will supersede any warranty conditions indicated in this manual that conflict with such laws.

22.2. ARTICLE 2 : TERMS OF REPLACEMENT

1. In case of INTENSIA failure because of a component failure, a production defect, or a conception error, occurring within two-year period starting from the implantation date, Sorin is committed to:
 - replacing free of charge the explanted device by a Sorin device with equivalent features,
 - or issuing a replacement credit equal to the purchase price for the purchase of any other Sorin replacement device.
2. After a two-year period and up to 4 years after the implantation, Sorin, because of limited warranty terms, will issue a replacement credit to the buyer of an amount equivalent to half of the initial purchase price minus prorata temporis during this two-years period.
3. In any case the credit issued by the limited warranty terms cannot exceed the purchase price of a Sorin replacement device.

23. PATENTS

The INTENSIA model described in this manual is covered by the following US patents:

5 167 224, 5 226 415, 5 271 394, 5 312 451, 5 325 856, 5 339 820, 5 350 406, 5 411 533, 5 462 060, 5 513 645, 5 545 181, 5 558 097, 5 564 430, 5 591 218, 5 626 619, 5 645 574, 5 674 265, 5 697 960, 5 702 424, 5 702 426, 5 713 928, 5 741 315, 5 776 164, 5 776 165, 5 818 703, 5 836 980, 5 868 793, 5 891 170, 5 891 184, 5 899 931, 5 931 856, 5 935 153, 5 954 660, 5 978 708, 6 181 968, 6 230 058, 6 236 111, 6 251 703, 6 256 206, 6 307 261, 6 337 996, 6 397 105, 6 408 209, 6 487 451, 6 487 452, 6 505 068, 6 532 238, 6 556 866, 6 604 002, 6 622 039, 6 625 491, 6 711 441, 6 738 665, 6 830 548, 6 889 080, 6 898 845, 6 912 421, 6 937 898, 6 975 905, 7 065 402, 7 072 716, 7 076 297, 7 113 826, 7 142 924, 7 164 946, 7 251 526, 7 366 566, 7 400 921, 7 400 922, 7 953 483.

24. EXPLANATION OF SYMBOLS

The symbols on product labelling have the following meaning:



Use by



Date of manufacture



Manufacturer



Serial number



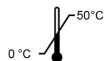
Batch number



For single use only.



Sterilised using ethylene oxide



Temperature limitation



High voltage



Consult instruction for use.



This icon is used to call your attention to a particularly important point.



This icon alerts you to a hazard that may result in equipment damage or personal injury. Carefully read the instructions provided with this icon.

FCC ID : YSGDR154

IC : 10270A-DR154

Last revision date of this implant manual: 2013-09

CAUTION: FEDERAL LAW RESTRICTS THIS DEVICE TO SALE BY OR ON THE ORDER OF A PHYSICIAN



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